Low-level Fall Simulation: Toddler Falling From Chair

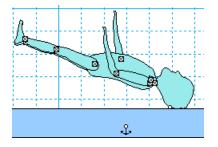
R. J. Reimann Professor Emeritus of Physics Boise State University 11 June 2012 (rev. 7/9/2013)

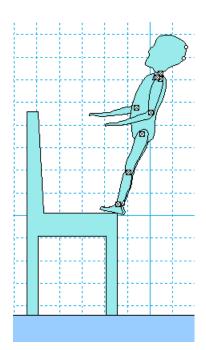
This simulation was generated using *Working Model*[™] software licensed at Boise State University for educational use only.

Situation

Toddlers occasionally fall from chairs or beds and hit their heads on the floor. They might simply lose balance and lean back too far or accidently step off attempting to regain balance. Resulting impacts have potential for grievous injury and even death.¹

> An extreme case occurs if the joints are frozen by fear or defiance and the head hits first. The model predicts an initial vertical impact speed $v_y = 4.5 \text{ m/s} \approx 10 \text{ miles/hour.}$ Note that this is almost $v_y = \sqrt{2gh} = 4.8 \text{ m/s}$ predicted by free-fall for the point simply dropping h = 1.2 mand the acceleration due to gravity $g = 9.8 \frac{m}{s^2}$.



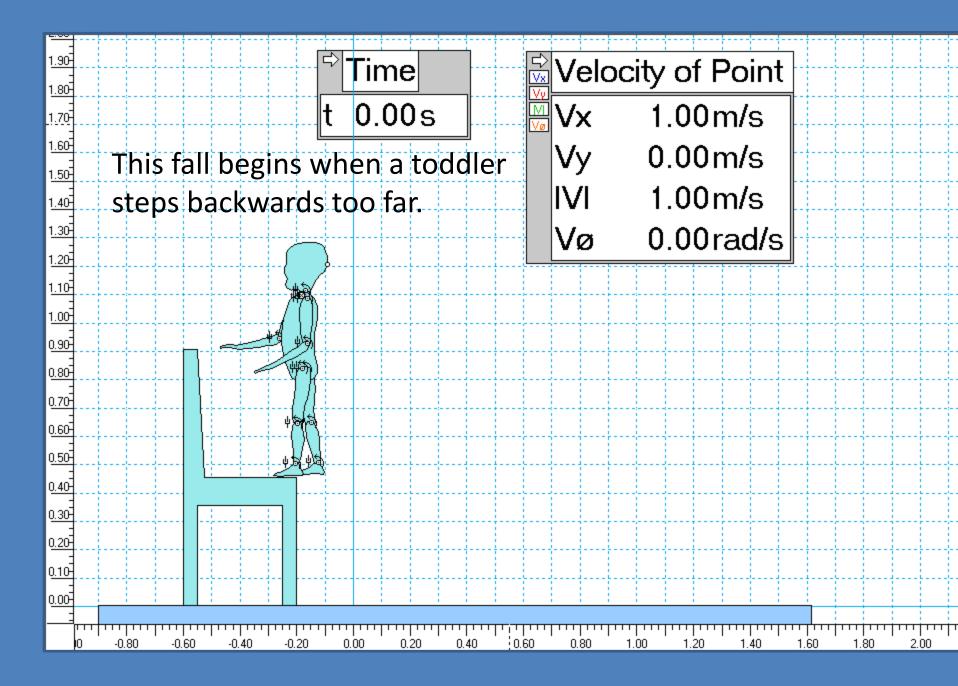


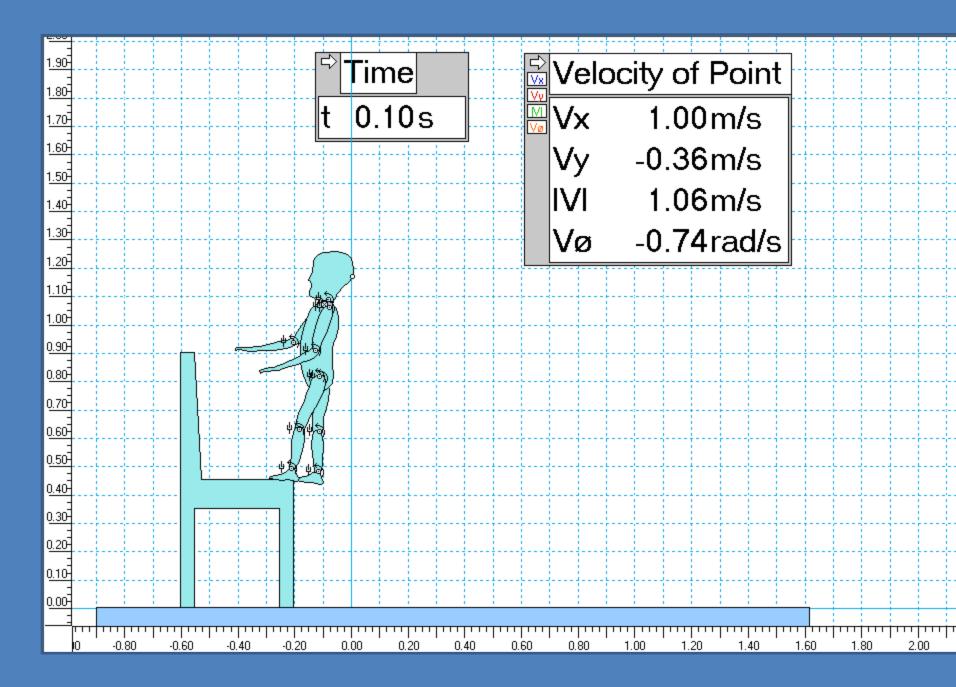
Refinements

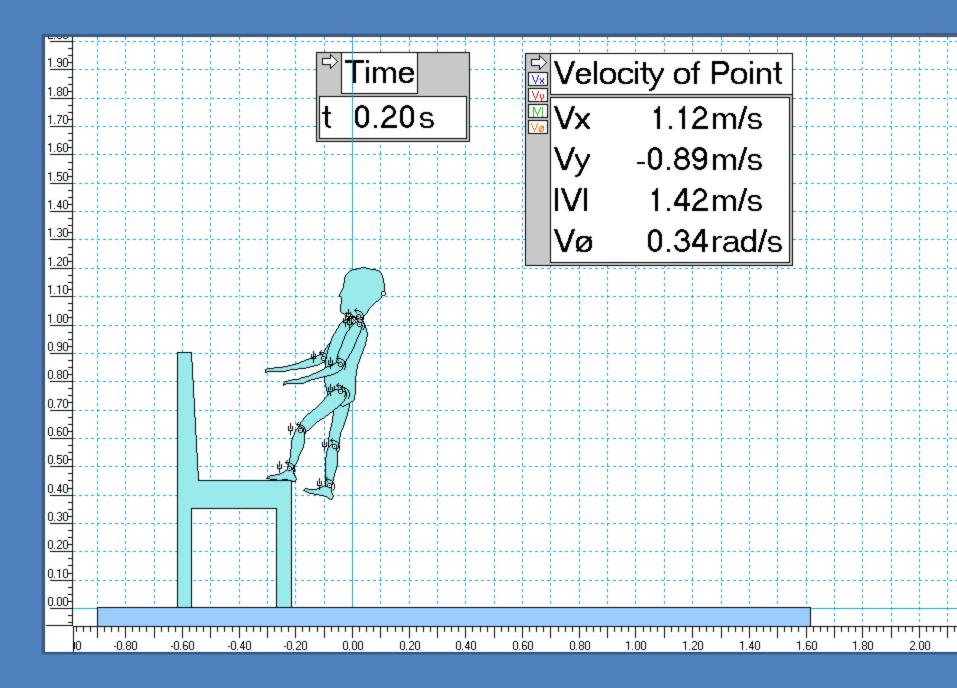
The following simulation allows flexible joints and other variable parameters to demonstrate one of countless possible scenarios between the previous rigid extreme and cases where the head does not even hit the floor. It is intended as a demonstration aid that is more realistic than an artist's conception.

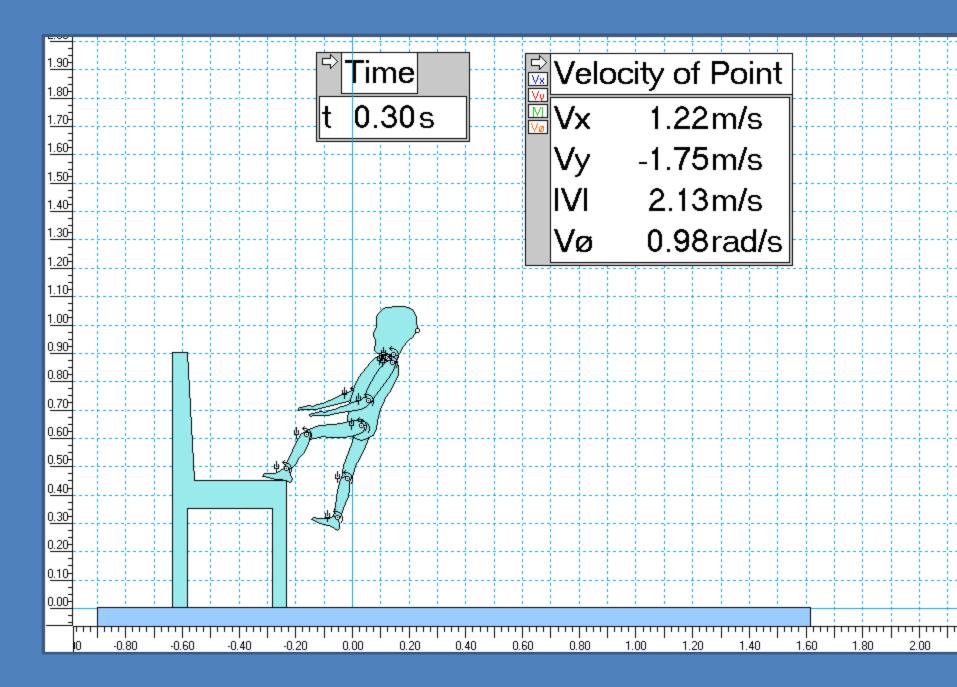
- An initial horizontal backwards step at 1.0 m/s is used and results in a first cranial impact speed of 5.4 m/s. This **exceeds** that predicted previously for free-fall, partly due to the initial speed.
- Derived results such as accelerations depend on contact time as explained in Appendix A.
- Prediction reliability is limited by the choice of model parameters given in Appendix B (mass distribution, joint approximations, elasticity and friction). Any changes to these parameters, initial posture, or rigidity of linked segments may change the outcome significantly.

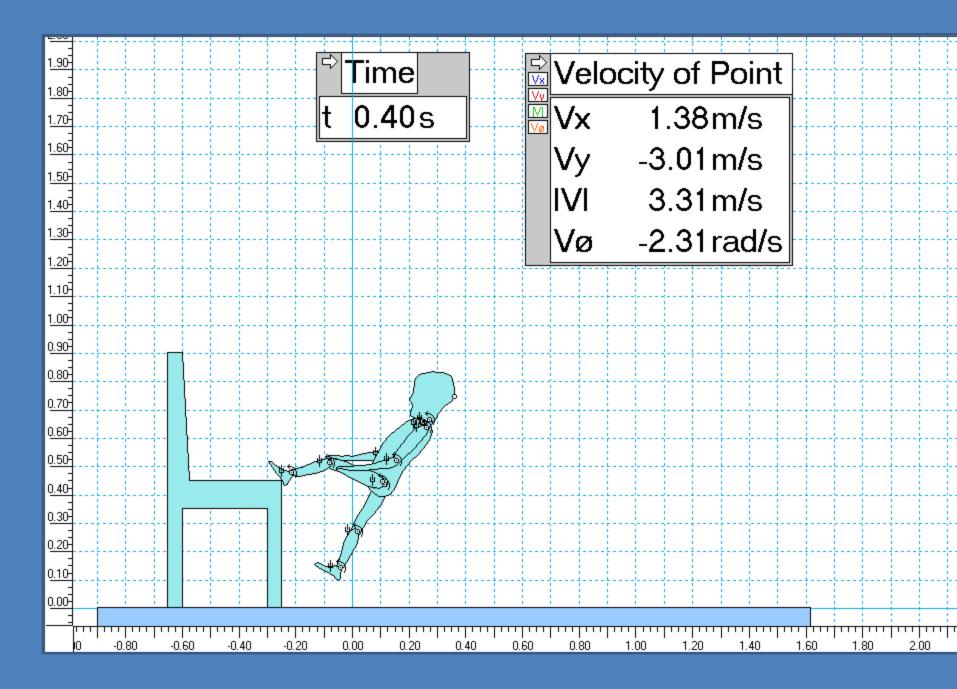
- The simulation is based on average dimensions for an 18-month old child crash-test dummy² with a stature of 0.81 m (32 inches) and mass of 11.0 kg (24.3 pound), including a 2.6 kg (5.8 pound) head. More details are given in Appendix B.
- Scale dimensions are in meters. Velocities are displayed for the initial cranial impact point. Multiply values in m/s by 2.24 to convert into miles/hour.
- The integrity of the software was checked by generating accurate predictions for cases with known analytical solutions. These were free-fall for a ball and toppling a long thin vertical rod about an ideal axis fixed at the bottom.
- Other computer simulations, physical models and video analysis are invited for comparison to help evaluate this simulation.

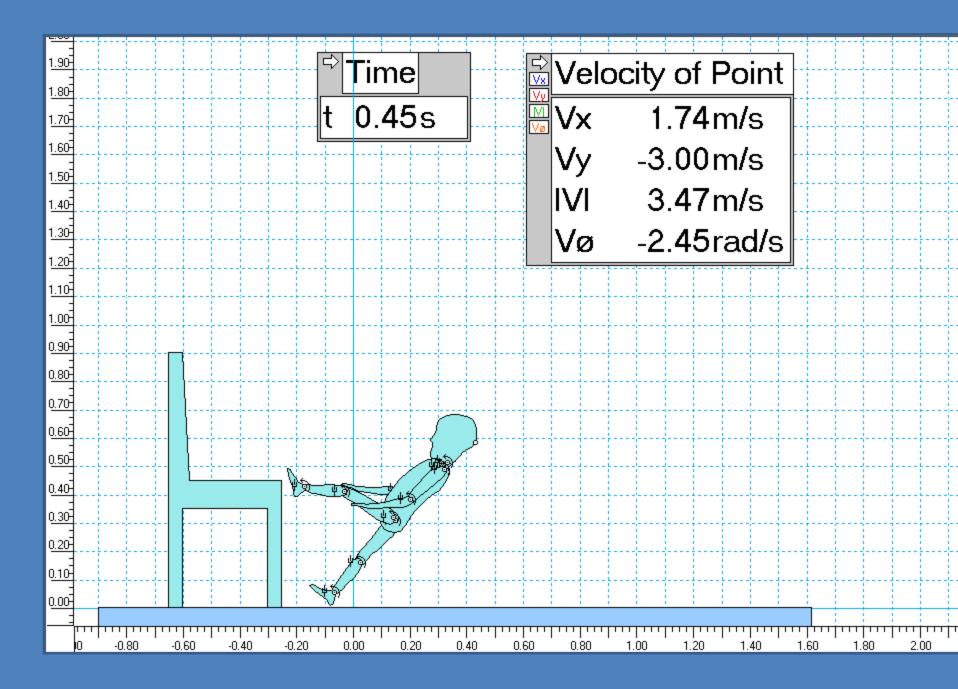


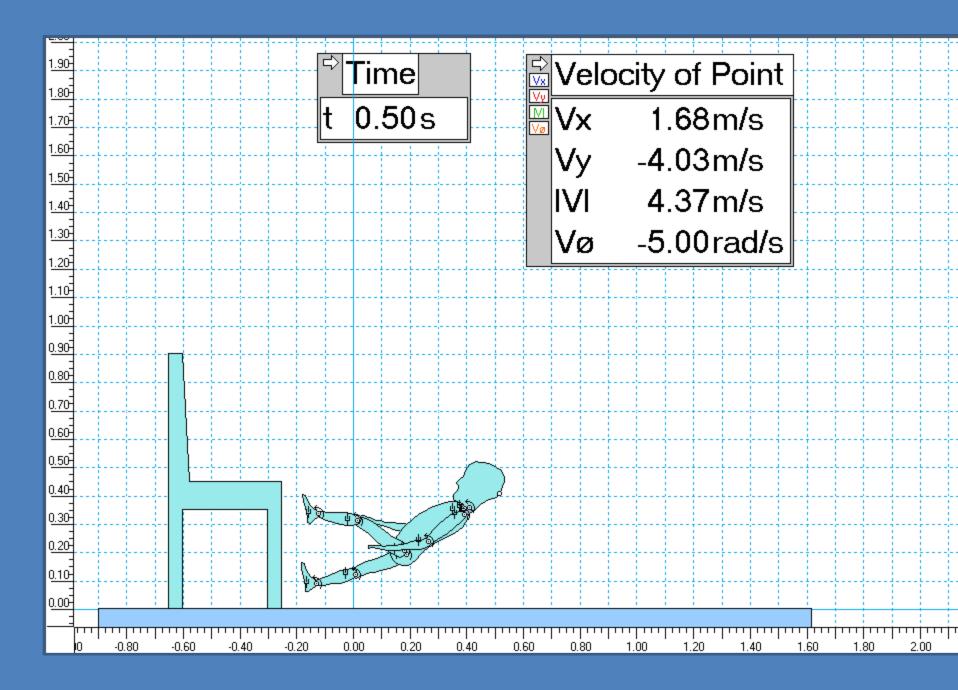


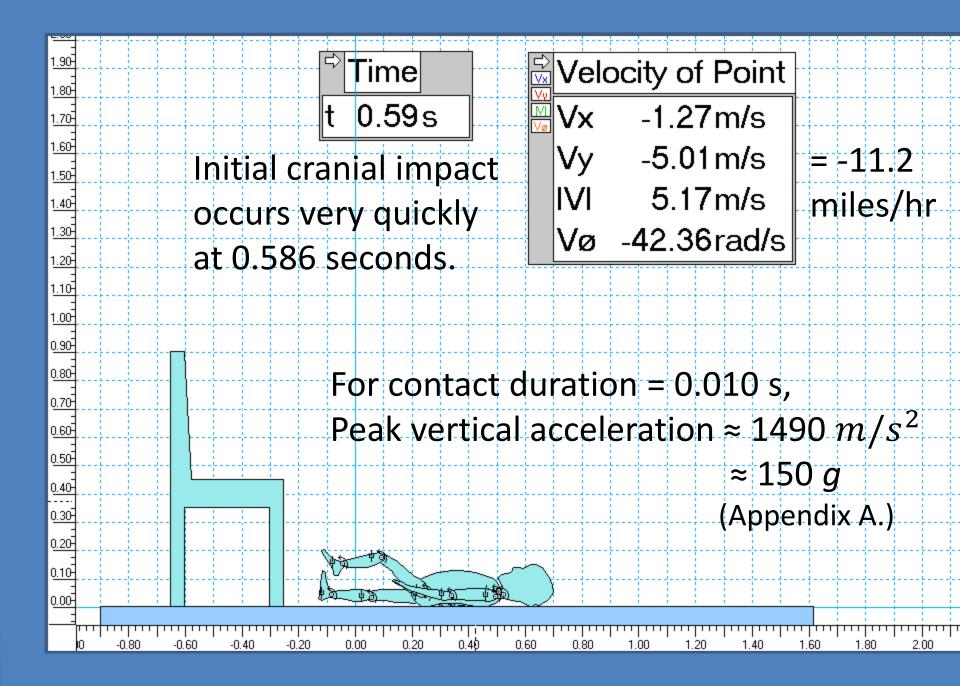


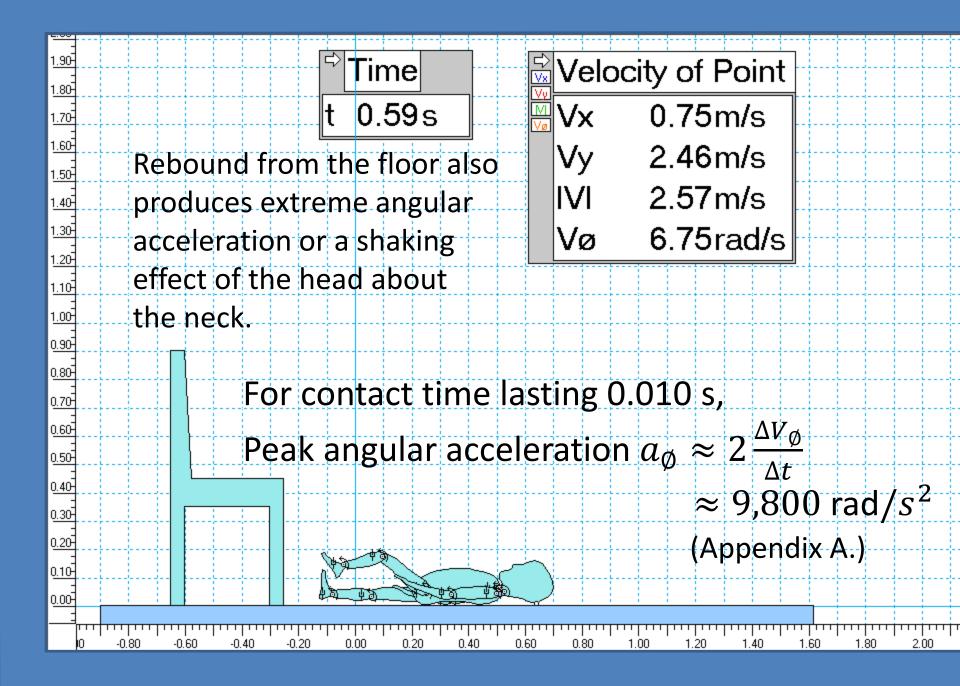


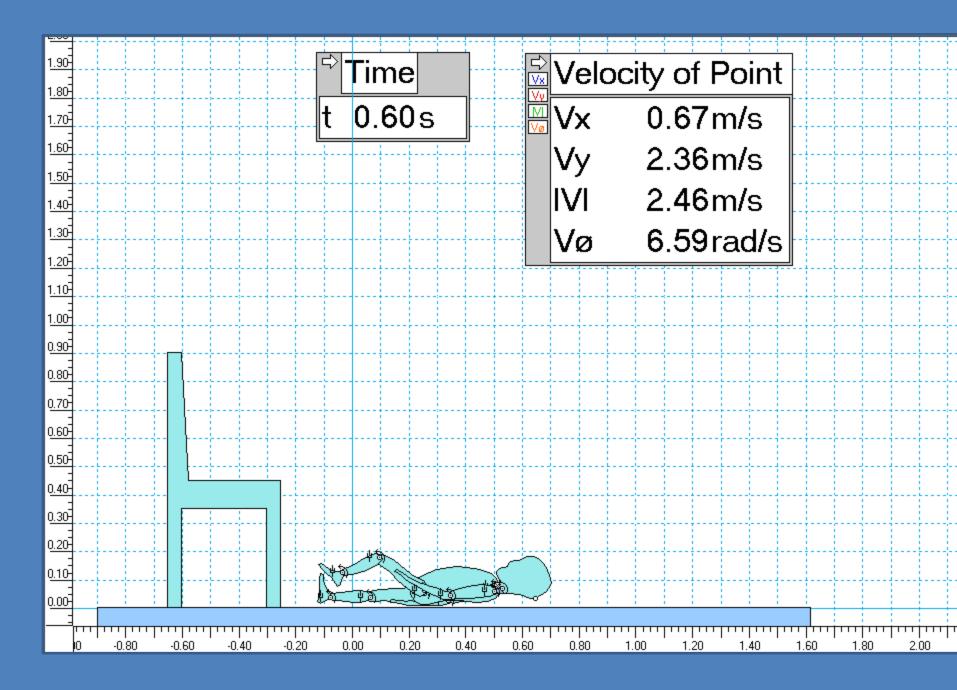


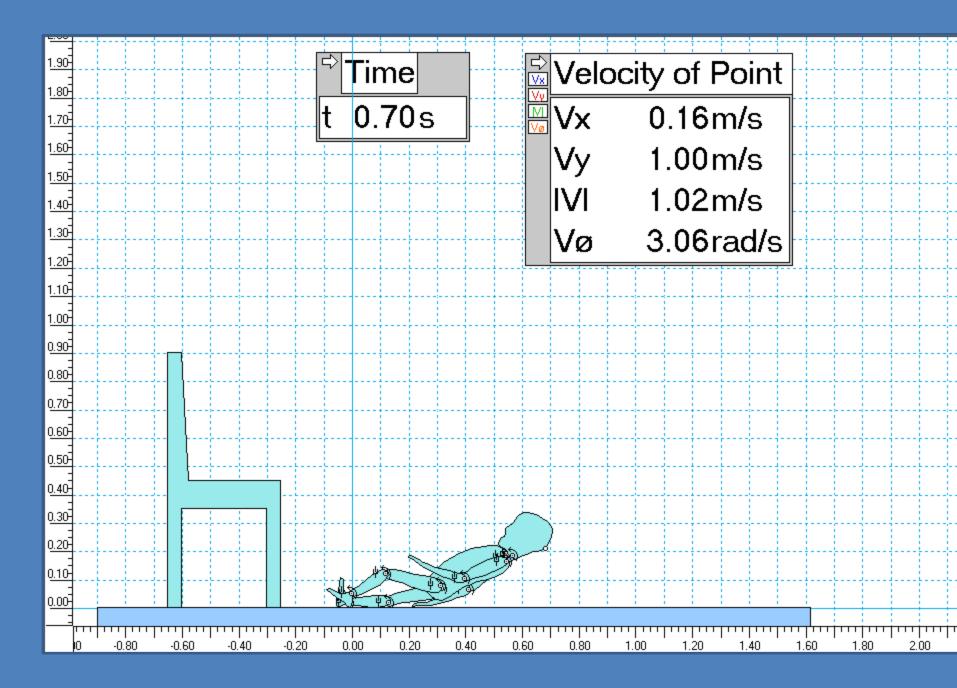


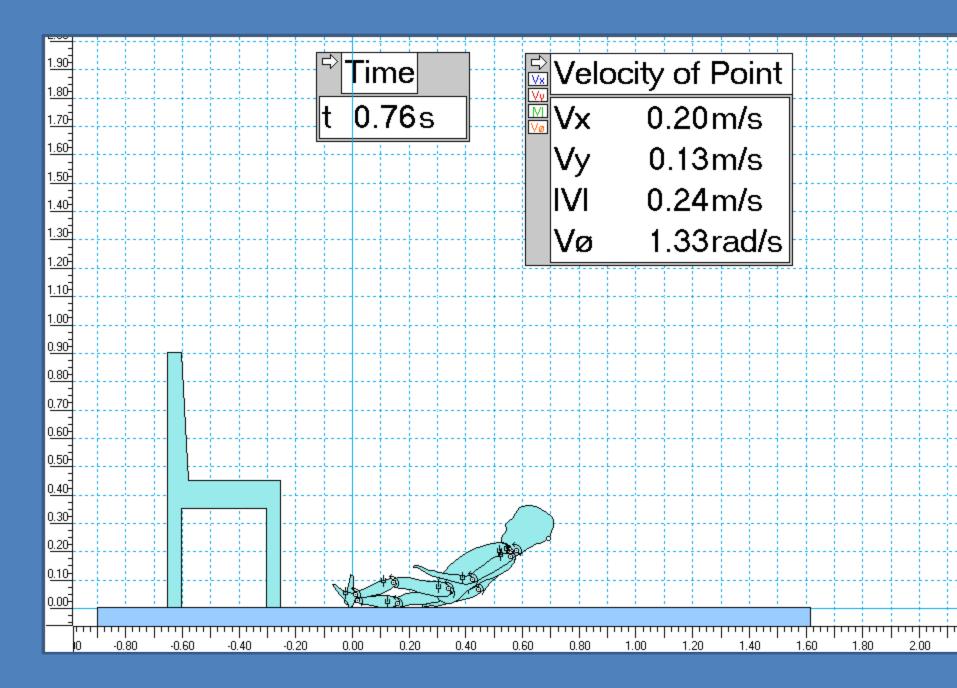


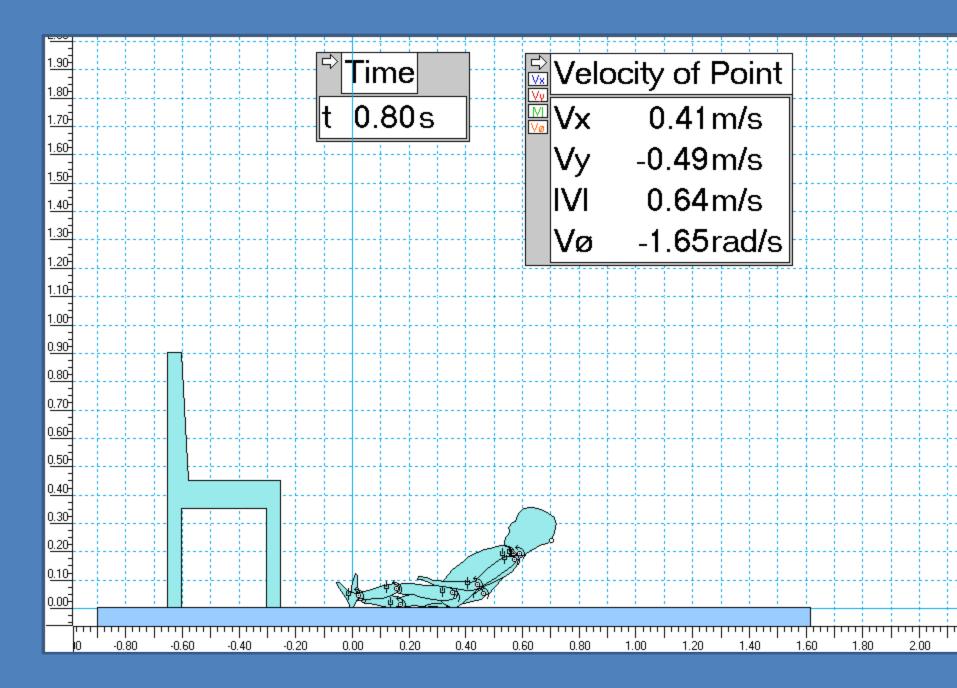


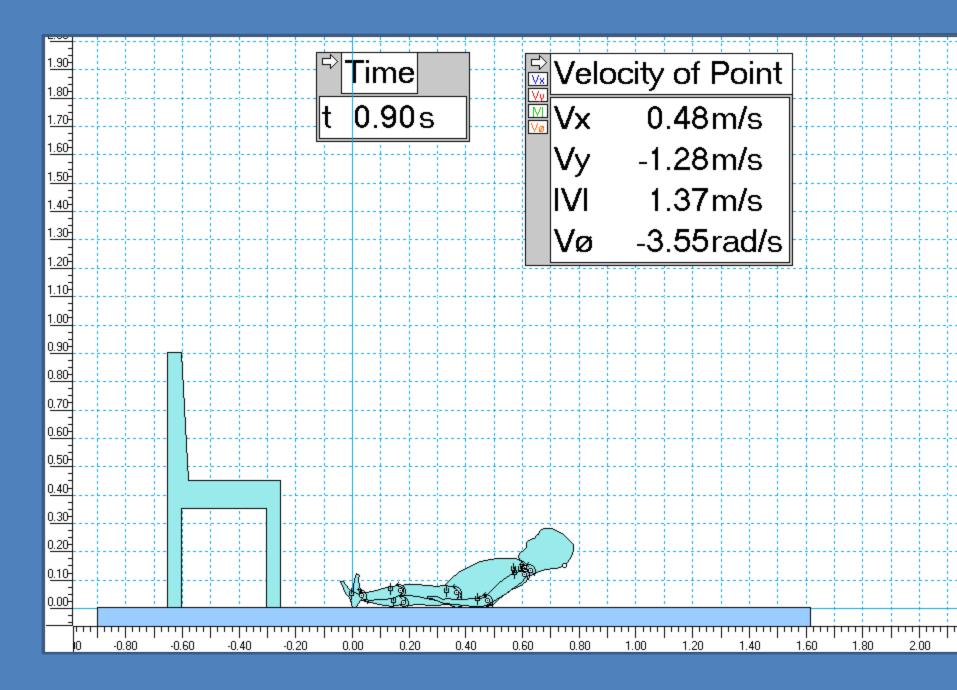


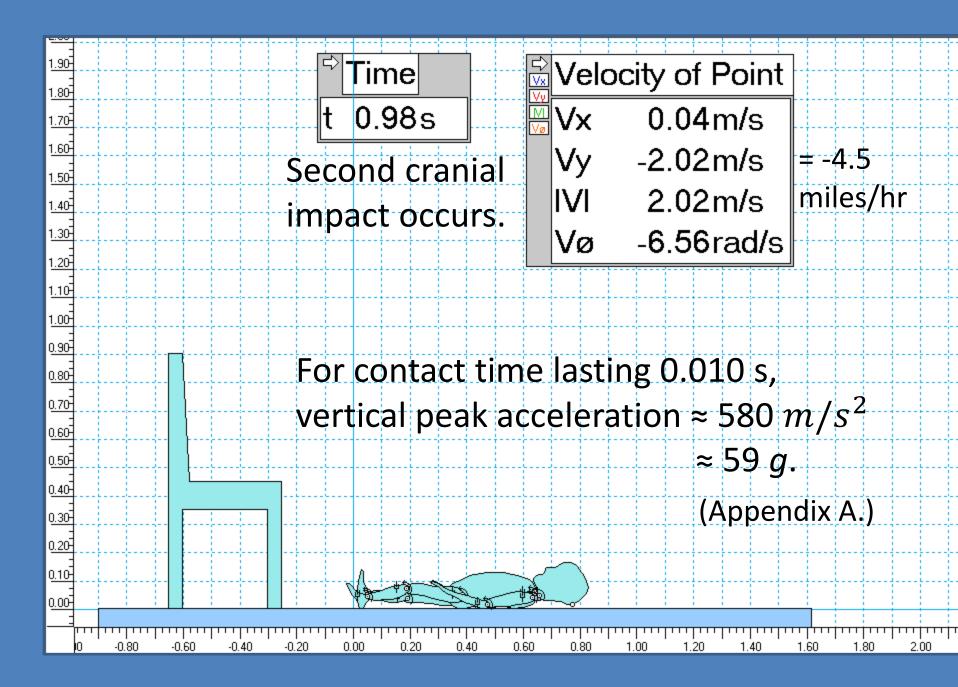


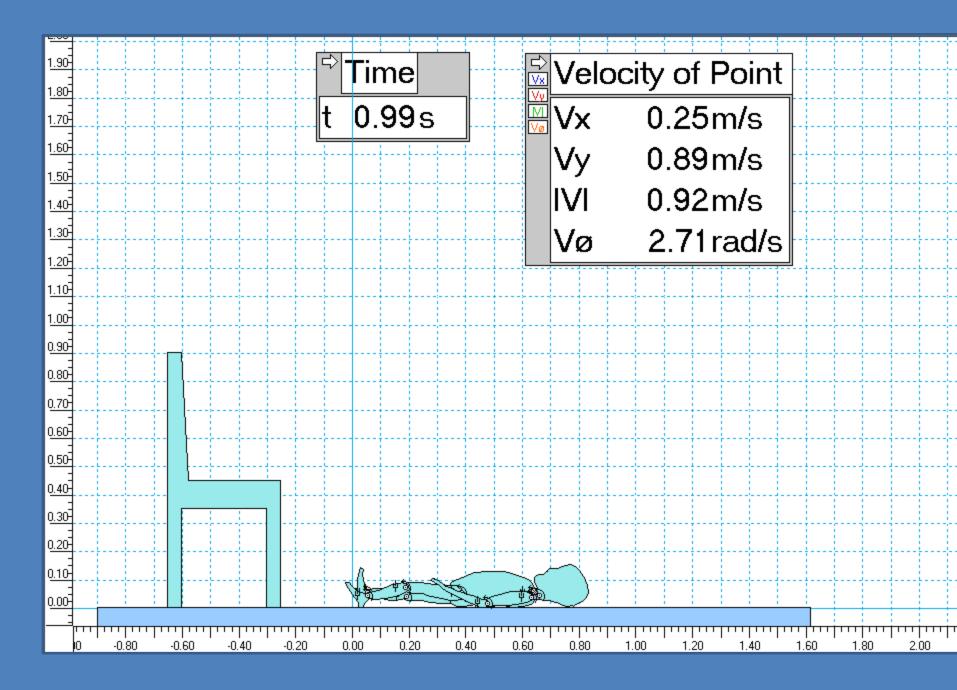


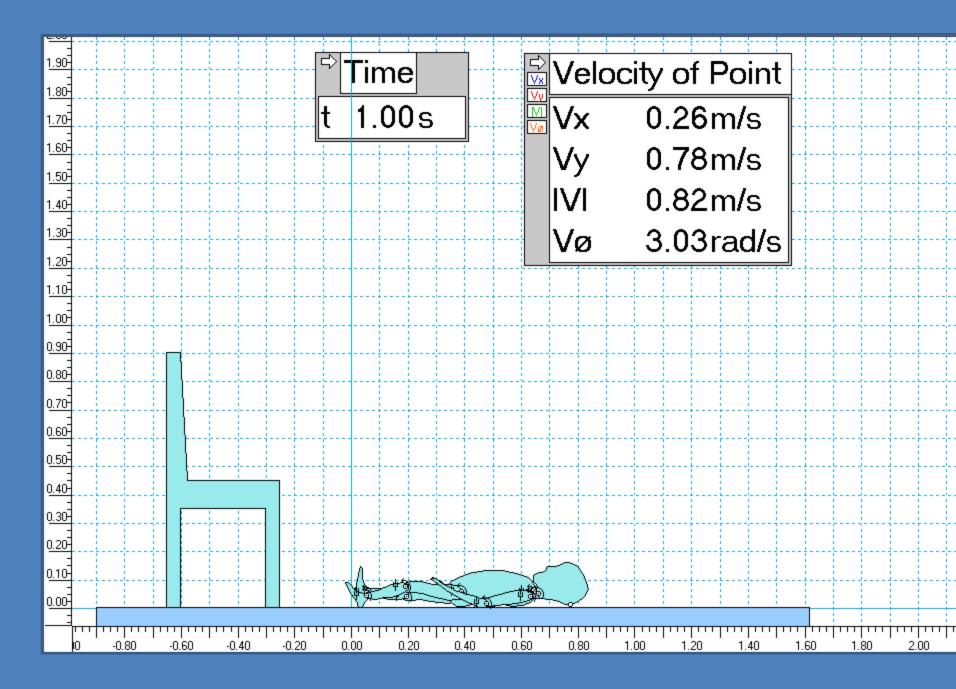


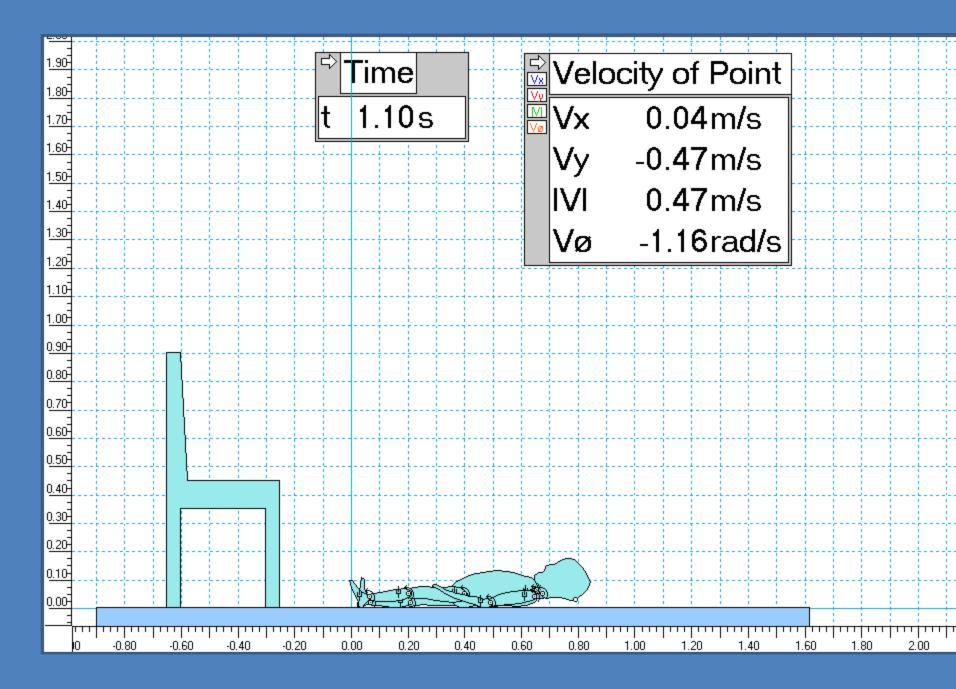


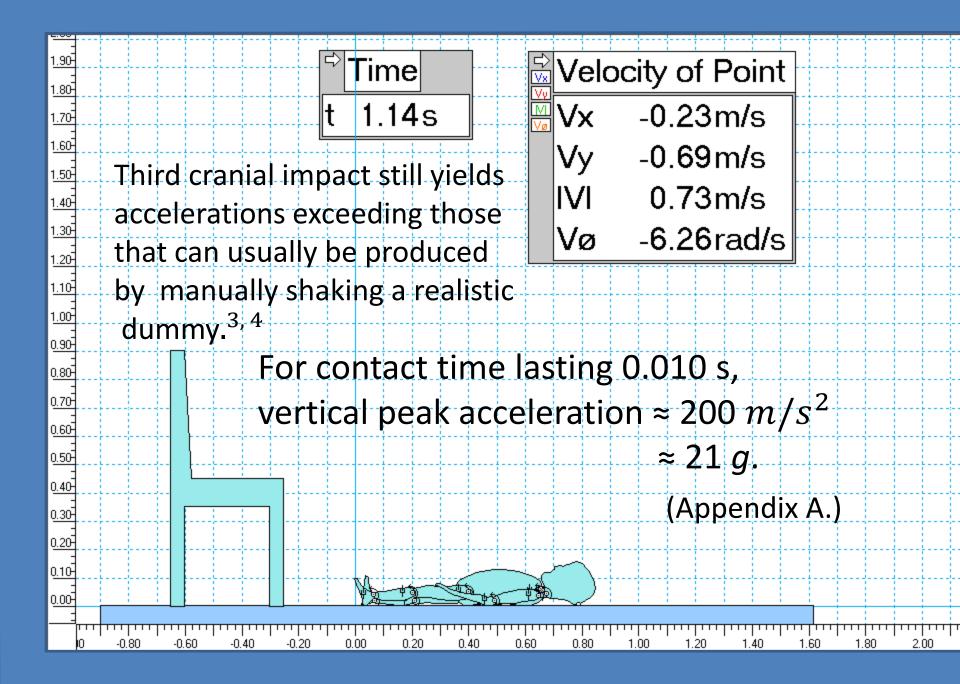




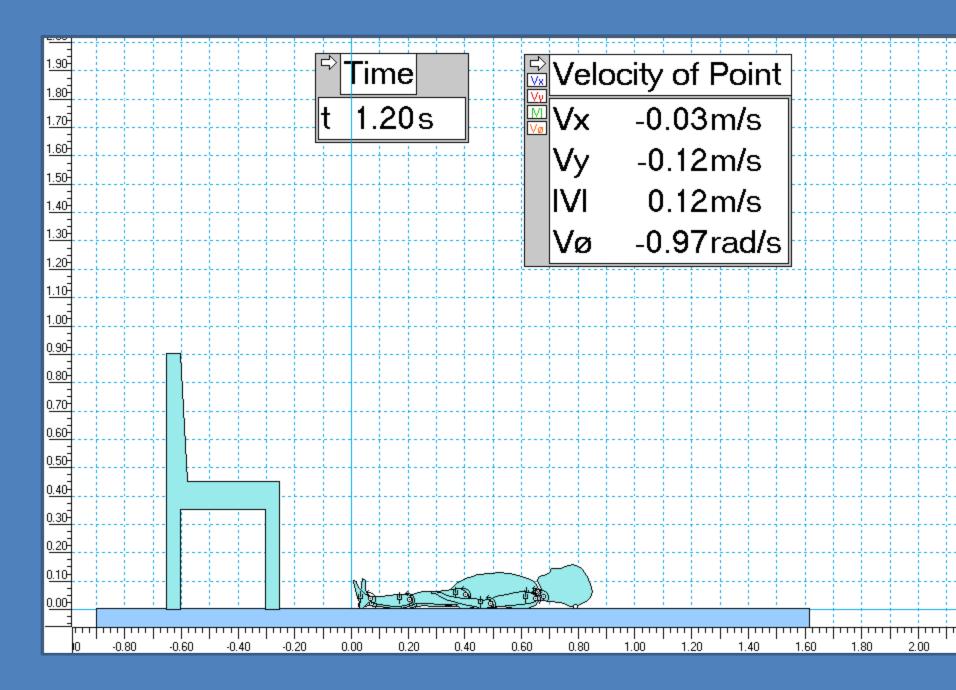


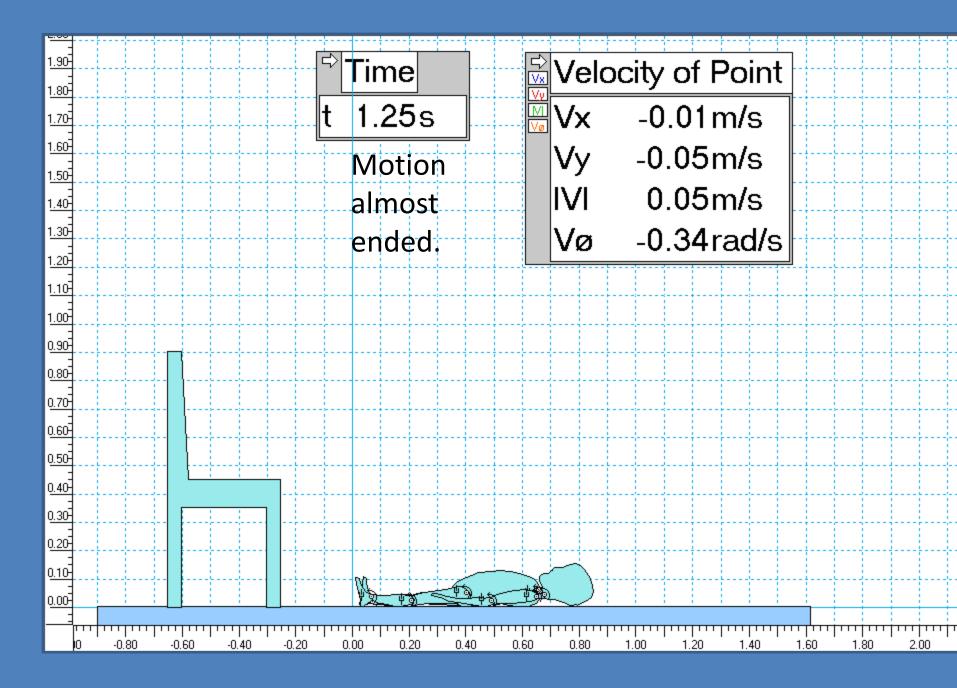






1 <u>.90-</u> 1.80-	Time					
1.70	t 1.15s	₩ Vx	0.14m/s			
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1.50-						
1.40-		IVI	0.36m/s			
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1 <u>.10-</u> 1.00-						
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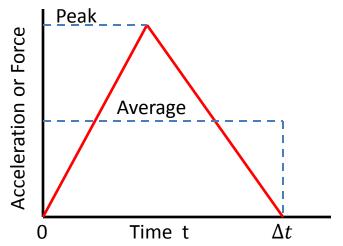


Conclusion

This simulation clearly shows the potential for severe head injuries from low-level falls. The resulting accelerations and forces for the first impact are more than 10 times greater than those that can usually be produced by manually shaking a realistic dummy.^{3, 4}

Appendix A. Physics Relationships

- By definition, the average acceleration in the vertical dimension $\langle a_y \rangle \equiv \frac{\Delta v_y}{\Delta t}$, where Δv_y is the change in velocity and Δt is the interaction time with the floor.
- A toddler head colliding with a rigid surface has $\Delta t \approx 0.005 \ s.^{3,4}$ Moderate padding extends this to $\Delta t \approx 0.020 \ s.$ $\Delta t = 0.010 \ s$ was chosen as a typical value.
- As illustrated, a linear approximation of the acceleration or force between the floor and the head shows that the maximum or peak value is about twice the average.^{4, 5}
- Divide accelerations in m/s² by g = 9.8 m/s² to convert into g's. Multiply accelerations by mass to convert into forces.



Appendix B. Model Specifications

 $(typical 18 - month old toddler)^2$

	Jo	oint	Rotational damping				
Body Segment	Mass (kg)	Percent			(N-m-s/rad)*		
Head	2.64	24.0	Н	Head-neck Shoulders Elbows	0.06		
Neck	0.38	3.4	S		0.13		
Torso	4.44	40.3	E		0.06		
Combined upper arms	0.64	5.8	F	Front Hip Back Hip Front Knee Back Knee	0.50 1.00		
Combined lower arms with hands	0.64	5.8	В				
Combined upper legs	1.13	10.3			0.10 0.60		
Combined lower legs	0.91	8.3	А	nkles	0.32		
Combined feet	0.23	2.1	* 0	*Detetional denominations de serve			
TOTAL	11.0 kg	100%	fc	*Rotational damping values chosen for realistic response since standards			
			are impossible for a variable organ				

- By definition, elasticity or coefficient of restitution ≡ |rebound velocity / impact velocity|.
 The head, arms, feet and floor are assigned values of 0.5, while the other segments are 0.1.
- All coefficients of friction = 0.30.
- Kutta-Merson with 0.001 second integration steps provides accuracy. Only about one step out of every hundred is illustrated.

References

- 1. Baker, Susan P., O'Neill, Brian, Ginsburg, Marvin J., and Li, Guohua. *The Injury Fact Book* (Oxford University Press 1992), 2nd ed., p.140
- 2. <u>http://www.humaneticsatd.com/crash-test-dummies/children</u>
- 3. Ommaya A K, Goldsmith W and Thibault L. Biomechanics and neuropathology of adult and paediatric head injury. British Journal of Neurosurgery 2002; 16(3): 220-242
- Goldsmith W and Plunkett J. A biomechanical analysis of the causes of traumatic brain injury in infants and children. The American Journal of Forensic Medicine and Pathology June 2004; 25(2): 89-100
- 5. Cross, Rod. The Bounce of a Ball. American Journal of Physics March 1999; 67 (3): 222-227